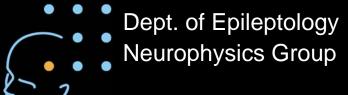
Physics in Brain Research

Klaus Lehnertz

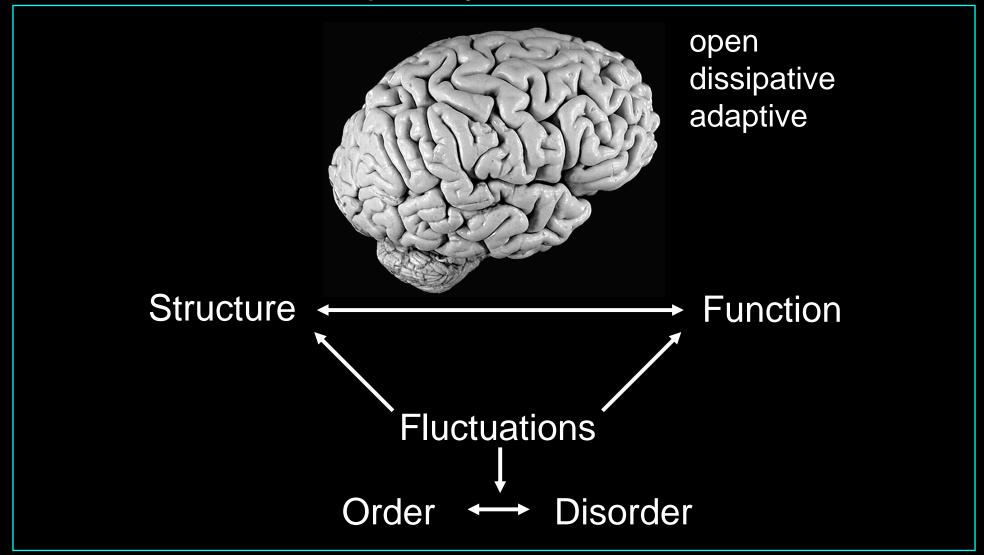


University of Bonn

Helmholtz-Institute for Radiation- and Nuclear Physics



Complexity of the Brain



Complexity of the Brain: Structure

number of neurons: $\sim 10^{10}$

number of synapses/neuron: $\sim 10^3 - 10^4$

total number of connections: ~ 10¹⁴

length of all connections: $\sim 10^7$ - 10^9 m

connectivity factor: ~ 10⁻⁶ (adult) - 10⁻⁴ (juvenile)

(number of connections present out of all possible)

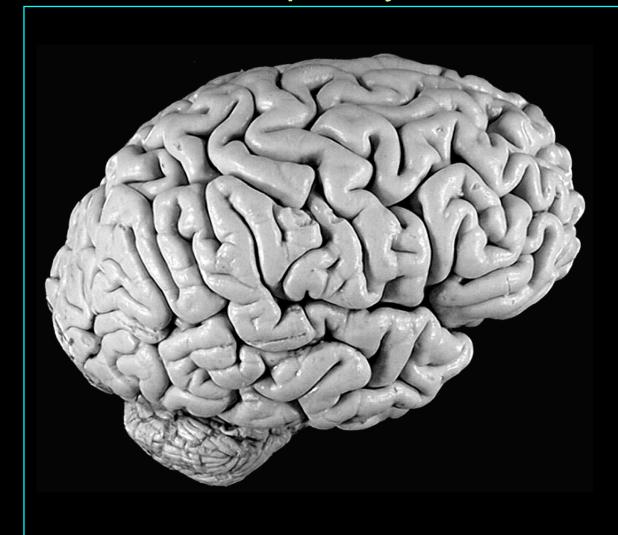
ion channel types / neuron $\sim 10^2$ - 10^3

neurotransmitter and other

active substances ~ 50

- brain networks are not random, but form highly specific patterns.
- neurons tend to connect with other neurons in local groups.

Complexity of the Brain: Function



control (body functions) movement perception attention learning memory knowledge emotions motivation language thinking planning personality self-identity consciousness dysfunctions

Understanding Functional and Structural Complexity of the Brain

non-destructive measurement of structure and function

of the living brain from the outside





Understanding Functional and Structural Complexity of the Brain

... requires multidisciplinarity !!

structure:

anatomy, histology, cytology, biochemistry, molecular biology, ...

function:

cognitive neurosciences, psychology, neurophysiology, electrophysiology,

physics+mathematicsengineeringcomputer science

Imaging Techniques in Brain Research

"passive" or "direct" imag	jing	"active" or "indirect" imaging			
measure signals generated by the brain	1	measure interactions between some appropriate energy and matter			
neuro- electricity magnetism		x-ray CT	PET	SPECT	nuclear magnetic resonance
el. fields mag. fields		μ	γ (511 keV)	γ	e. m. fields HF
function / (morphology)		morpholog	y metabo	olism	function / morphology
EEG MEG ECoG, SEEG LFP, AP, MP			PET-CT		MRI, fMRI MRS DTI

Historical overview

1895	Discov	erv of	x-ravs
		- - - -	

1946 NMR principles

1948 Nuclear medicine scan

1952 Ultrasound imaging

1953 Positron tomography

1971 Single Photon Emission

Tomography

1972 Development of x-ray CT

1976 NMR Imaging

Nobel Prizes

- Röntgen (1901, x-rays)
- Rabi (1944, MR)
- Bloch, Purcell (1952, MR)
- Hounsfield, Cormack (1979, CT)
- Ernst (1991, NMR)
- Wuthrich (2002, NMR)
- Lauterbur, Mansfield (2003, MRI)







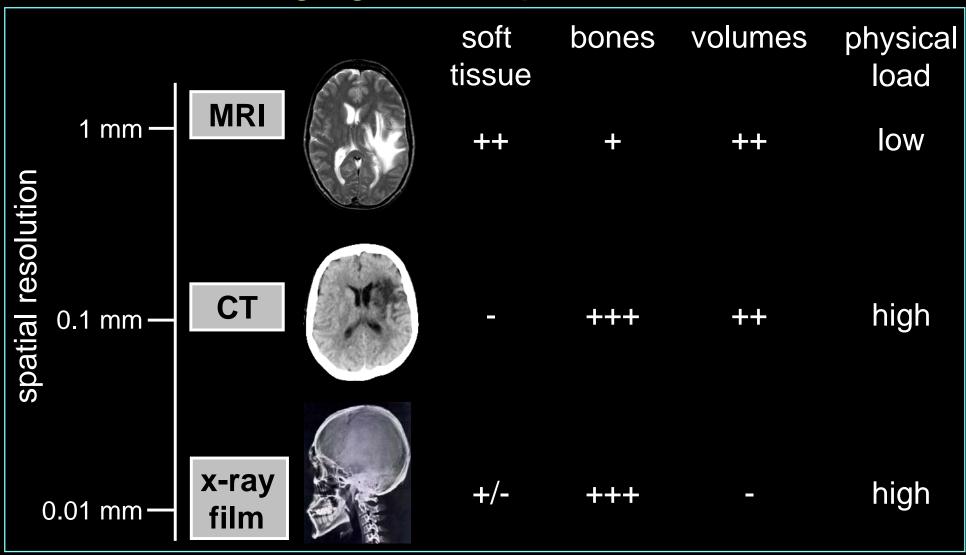












Limiting factors

Physical limits

x-ray/CT: number of γ-quanta

MRI: proton density/volume

Technical limits

x-ray/CT: tubes, detectors, ionizing radiation

MRI: field strength, coils

Noise, Artifacts

Possible improvements

Measurement techniques

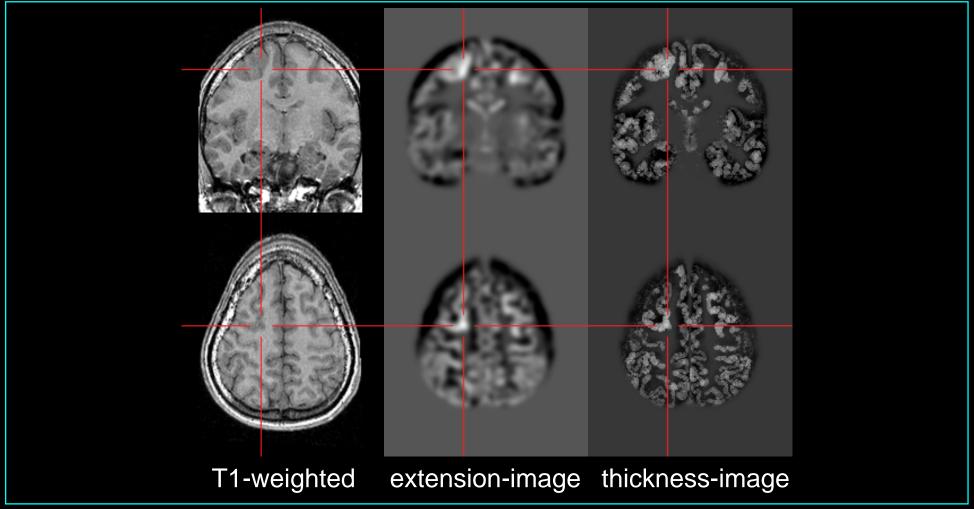
Advanced post-processing techniques

Contrast agents, magnetic nanoparticles, ferrofluids

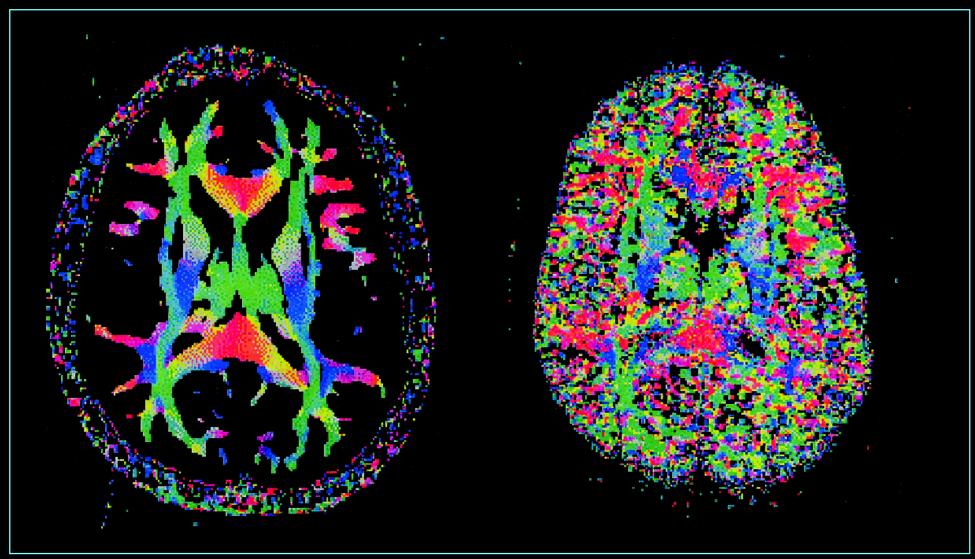
Combined techniques (PET-CT, PET-MRT)

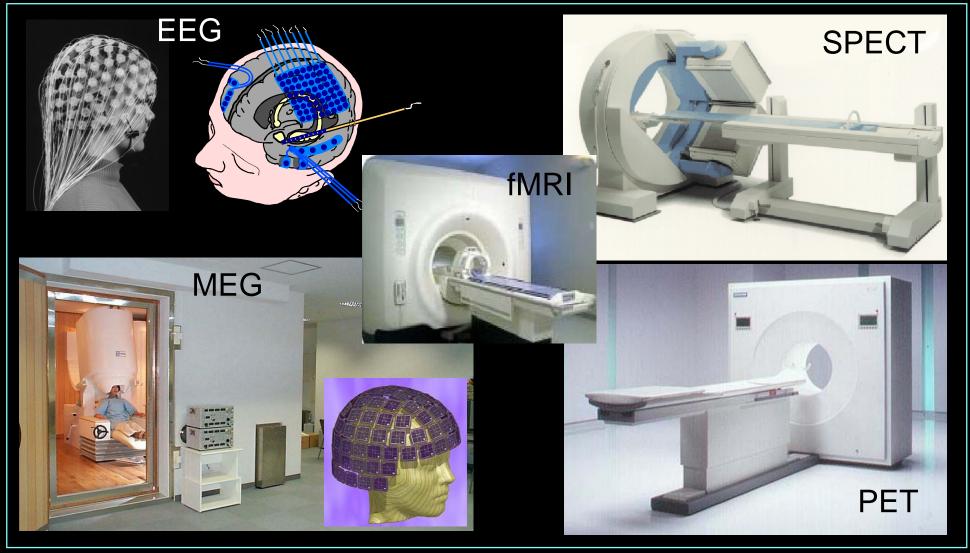
Structural Imaging in Focal Cortical Dysplasia

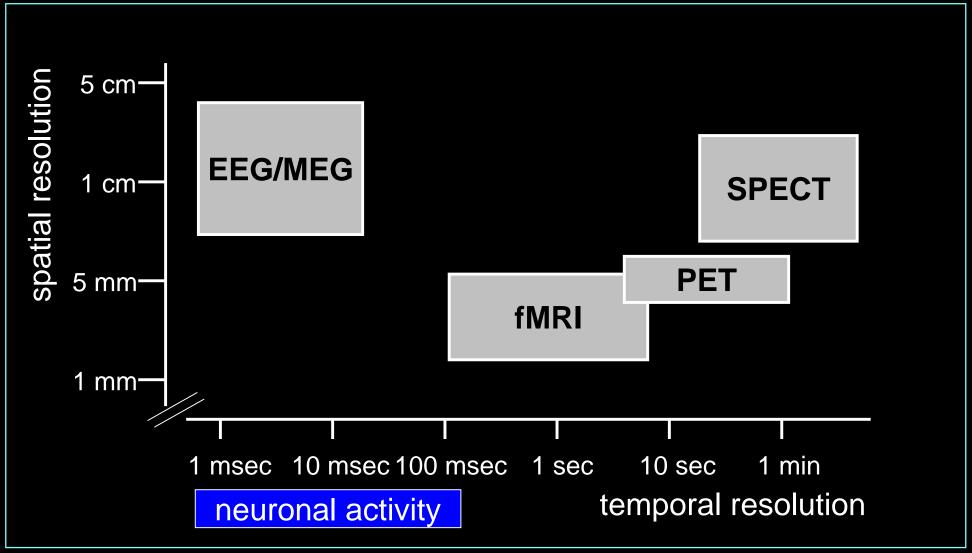
- Visualization of Blurred Gray-White Matter Junctions -



Fiber Tracking with Diffusion Tensor Imaging







- Measurement Techniques -

neuronal activity	spatial res	olution	temporal resolution
direct measurements - single/multiple unit recordings - local field potentials (LFP) - stereo-electro-	high	eness	high
encephalogram (SEEG) - electrocorticogram (ECoG) - electroencephalogram (EEG) - magnetoencephalogram (MEG	low	invasiveness	
indirect measurements - PET / SPECT - fMRI	low high		low

Functional Imaging

Specific Aims

- analysis of information processing in the brain
- alterations due to pathologies of central nervous system

temporal information: what, when, and why?

spatial information: what, where?

- modeling, prediction

Historical overview

1929	electroence	phalogram

1947- evoked potentials

1953 Positron tomography

1971 Single Photon Emission

Tomography

1975 magnetoencephalogram

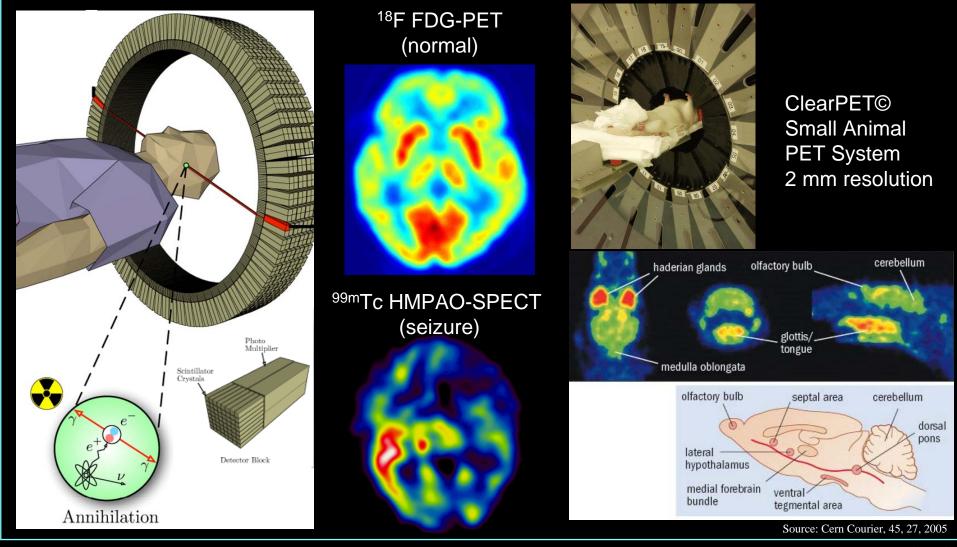
1976 NMR Imaging

1990 BOLD-Effect

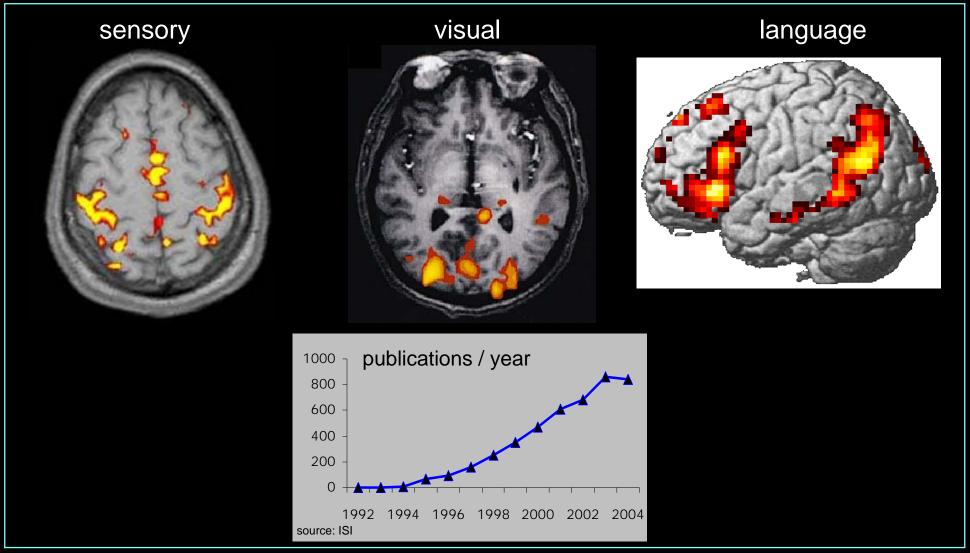
Nobel Prizes

- Sherrington, Adrian 1932 function of neurons
- Eccles, Hodgkin, Huxley 1963 ionic mechanism in neurons
- Bardeen, Cooper, Schrieffer 1972 superconductivity
- Sperry, Hubel, Wiesel 1981 information processing visual system
- Lauterbur, Mansfield 2003 magnetic resonance imaging

Functional Imaging Techniques: PET/ SPECT



Functional Imaging Techniques: fMRI



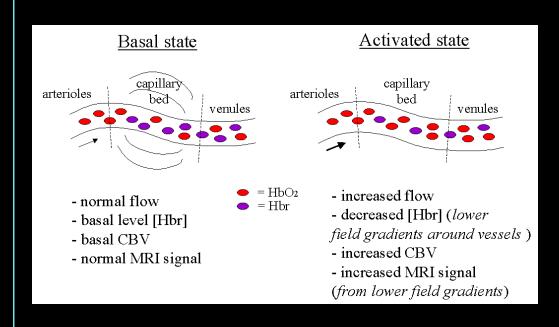
Functional Imaging Techniques: fMRI

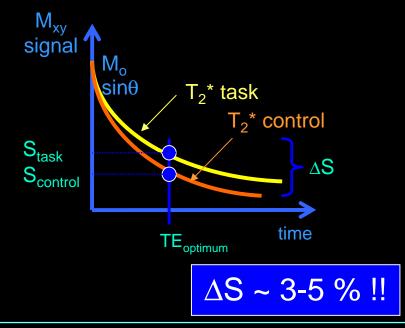
IDEA: use Hemoglobin (Hgb) as *intrinsic tracer*.

- oxy-Hgb is diamagnetic, deoxy-Hgb is paramagnetic (local field inhomogeneities)

BOLD (Blood Oxygen Level Dependent) Effect:

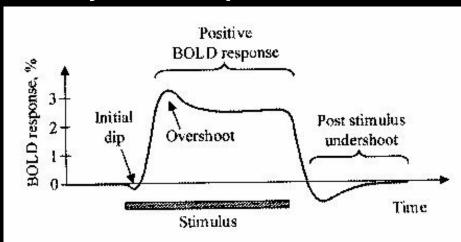
↑neural activity → ↑ blood flow → ↑ oxy-Hgb → ↑ T2* → ↑ MR signal





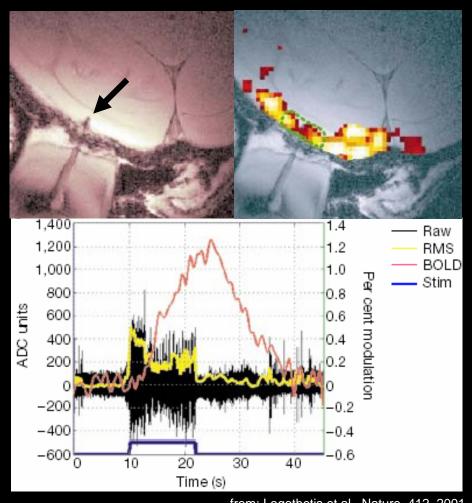
Functional Imaging Techniques: fMRI

hemodynamic response function

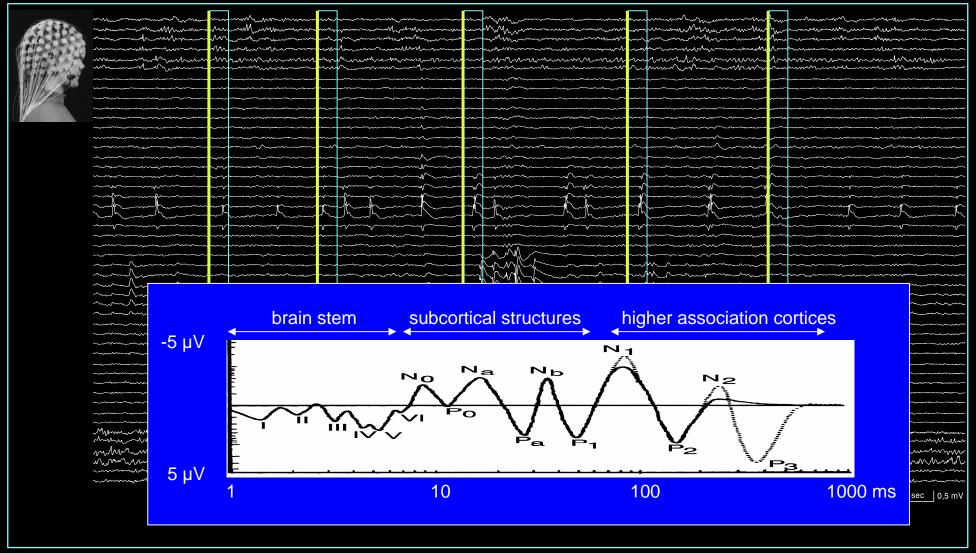


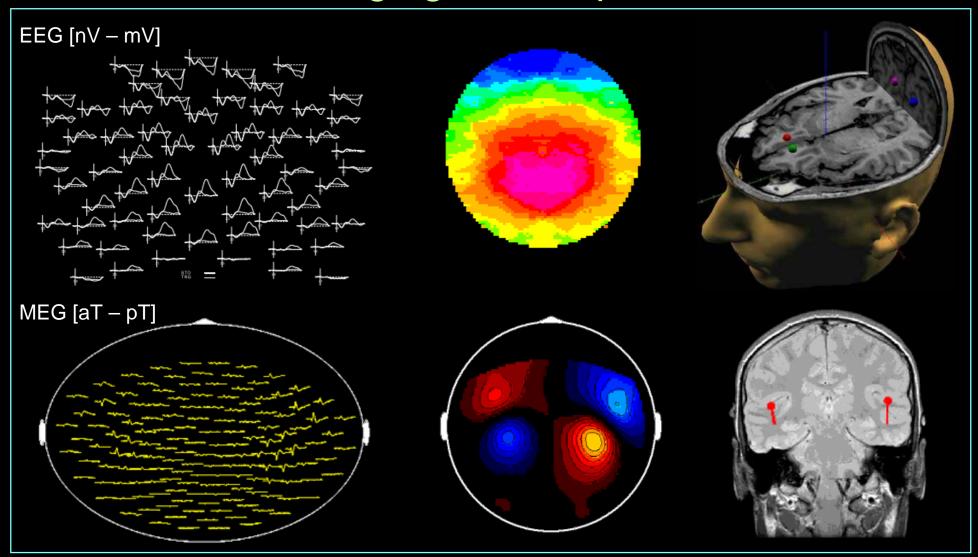
BOLD-effect and neuronal activity:

- monotonous but nonlinear relationship
- neurovascular coupling?
- initial dip?
- time scales?

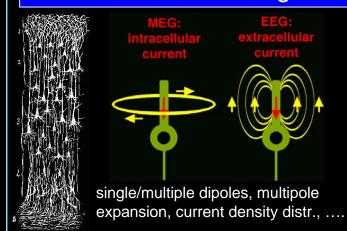


from: Logothetis et al., Nature, 412, 2001





source modeling



volume conductor modeling

half space sphere ellipsoid realistic models

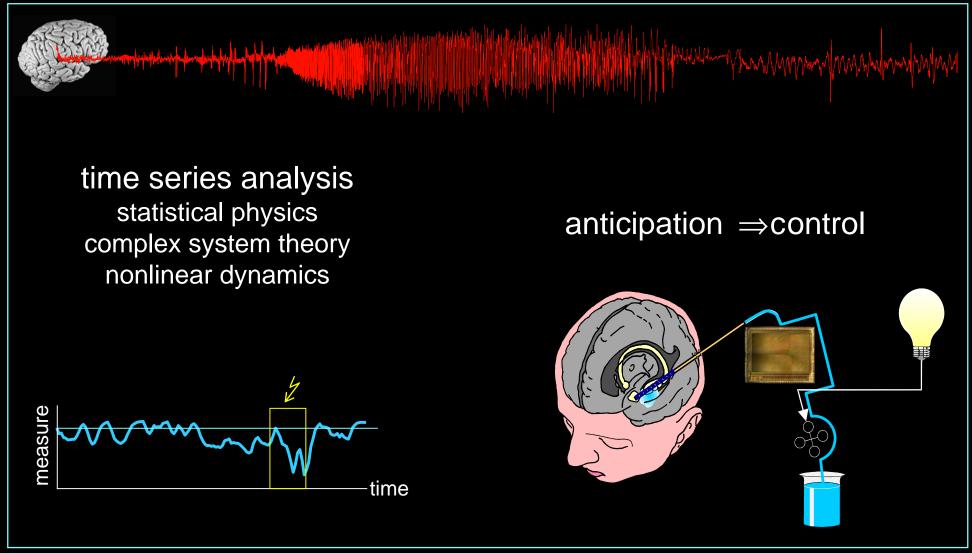


inverse problem

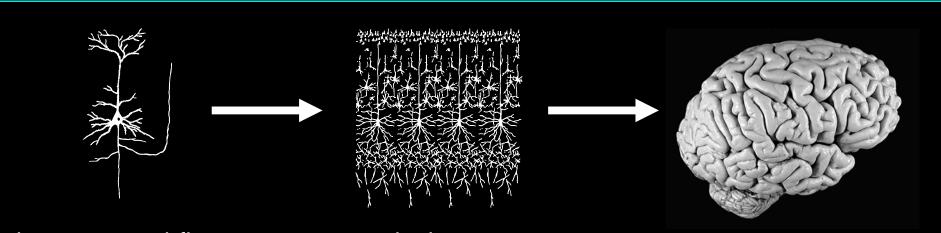
$$\vec{B}(\vec{r}) = \frac{\mu_0}{4\pi} \int j(\vec{r}') \times \frac{\vec{r} - \vec{r}'}{|\vec{r} - \vec{r}'|^3} dr'$$

$$V(\vec{r}) = \frac{\sigma_0}{\sigma_{\vec{r}}} V_0(\vec{r}) - \frac{1}{4\pi} \sum_{i,j} \frac{\left(c_i - c_j\right)}{\sigma_{\vec{r}}} \int_{S_{i,i}} V(\vec{r}') \frac{\left(\vec{r} - \vec{r}'\right)}{\|\vec{r} - \vec{r}'\|^3} x dS' \qquad V_0(\vec{r}) = \frac{1}{4\pi\sigma_0} \int \frac{\nabla' \cdot j(\vec{r})}{\|\vec{r} - \vec{r}'\|^3} dv'$$

3D localization of neuronal activity



Understanding Functional and Structural Complexity of the Brain: Modeling



integrate-and-fire FitzHugh-Nagumo Hodgkin-Huxley

ion channels neurotransmitter synapses

branching structure

network size connectivity

inhibition/excitation feed back/ feed forward coupling

interneurons / glia cells



Understanding Functional and Structural Complexity of the Brain

medical/biological physics

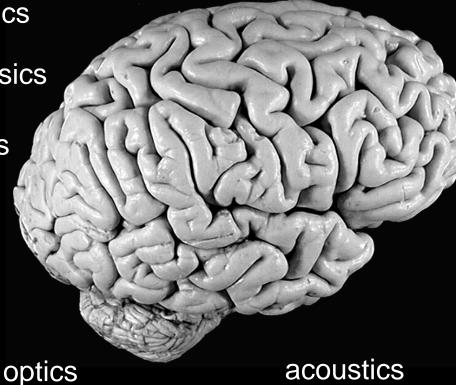
statistical physics

computational physics

nonlinear dynamics

thermodynamics

electrodynamics



condensed matter physics

low temperature physics

detector physics

nuclear/atomic physics

Understanding Functional and Structural Complexity of the Brain

Medical imaging celebrated its centennial anniversary in 1995, and today it continues to push the frontiers of research and clinical applications forward. It is an excellent example of what can be done through a multidisciplinary effort, in this case involving physicists, engineers, and physicians.

Many research opportunities are available, as much remains to be done in further improving the applications of medical imaging to reducing human disease and disability.

W. R. Hendee Physics and applications of medical imaging Rev. Mod. Phys., Vol. 71(2), pp. S444, Centenary 1999

How to Reduce Noise

- Head motion artifacts are the worst
- Test experienced subjects
- Give your subjects clear instructions (e.g., try not to swallow)
- Consider motion correction algorithms (Jody's opinion: garbage in, garbage
- •out, when in doubt throw it out; exception: rare subjects such as patients)
- Spatially smooth the data
- Tradeoff: lose resolution
- •• Choose your signal power in a frequency with low noise
- high noise at low frequencies (so don't use long epochs: optimum epoch
- duration is 16 sec)
- - try to have multiple repetitions of conditions within each run
- high noise at breathing frequency (once every 4-10 seconds)
- •• Temporal smoothing
- At a minimum, perform linear trend removal
- Consider filtering out low frequencies (high-pass filter)
- Jody advises against filtering out high frequencies (temporal Gaussian)
- because it artificially inflates your stats

- •Go with a stronger magnet (4T rules!)
- •• Go with a better coil (surface coil)
- Tradeoff: lose other areas
- •• Take bigger voxels
- - Tradeoff: lose spatial resolution, if voxels are too big, you
- •lose signal
- •• Make sure your subject is paying attention to the
- •stimuli/task
- - e.g., "1 back" task: hit button after every stimulus repetition
- - Tradeoff: Attention itself can distort the activation
- Caveat: need to be sure attention is comparable across
- conditions